

# ELECTROCARDIAC DEFIBRILLATION MODELING

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# **Motivation**

#### — Cardiac Fatal Diseases

- Sudden cardiac death (SCD): unexpectedly, spontaneously death from heart arrest.
- Ventricular fibrillation (VF): uncoordinated contraction of the muscle of the ventricles.
- Fibrillation is a turbulent electrical state, causing death if not treated.





Normal sinus rhythm





## Defibrillation — Treatment for fibrillation

- Strong electrical shock
- Electrical shock/heart boundaries
  - gives virtual electrodes
- Resets the electrical wave of the heart to its normal routine.



# Goals

- Understand role of virtual electrodes in terminating fibrillation.
  - Defibrillation simulations
  - Analysis of filaments interacting with virtual electrodes
- LEAP as well as normal defibrillating voltages



# Main Results

- Defibrillation electrical shock creates the virtual electrodes in realistic heart geometry.
- Virtual electrodes appears primarily near the epi/endocardium cardiac surfaces and large blood vessels play a secondary but still important. However, small blood vessels appear to have smaller role.
- Strong shock defibrillation extends polarized region to terminate fibrillation.
- LEAP defibrillation:
  - Extensive filament motion during LEAP as possible contributor to LEAP defibrillation.
- Sensitivity of the simulations to the conductivity values and blood vessel walls.

# **Resources for Computing**



- LIred and Handy cluster (IACS at SBU)
  - 8 hours using 192 processors for 10ms defibrillation simulation
- Possible role of GPU speed up, collaborating with cyber heart community as chaste upgrade.

# CyberCardia

# **Defibrillation Modeling**

Chaste

- Bidomain with a Bath problem
- finite element method
- Two currents added to Chaste
  - Electroporation
  - Asymmetric response
- Blood vessel wall model (inter/outer wall)



#### Cardiac Model for Defibrillation Simulation — Bidomain Model

- Most complete computationally tractable cardiac tissue model.
- Explicit account for both extracellular and intracellular domains.
- Able to model unequal anisotropy ratios and defibrillation.



 $\phi_i, \phi_e$ : intracellular, extracellular potential  $V_m$ : transmembrane voltage  $V_m = \phi_i - \phi_e$ 



### Cardiac Model for Defibrillation Simulation — Bidomain with a Conductive Bath

- Solution domain  $\Omega = \mathbb{H} \cup \mathbb{T}$ .
- Perfusing bath region  $\mathbb{T}$ .
- Bath potential  $\phi_t$  in  $\mathbb{T}$
- Electrodes act on the bath boundary only.





#### Oxford Rabbit Heart – High Resolution cyber Tetrahedral Mesh (40M) Reconstructed from MRI data





# Blood vessels of Rabbit heart from Chaste tetrahedral mesh (left) vs. Rat vasculature (right)





#### Isotropic simulations with Rat and Rabbit





#### Defibrillation Simulation —Bidomain with Bath Problem



- Computational domain (2.4x2.4x3.2cm) in a model of cardiac tissue contained in a conductive bath.
- The color represents transmembrane voltage and the Initial voltage is -83 mV.
- Use of physiological parameters.
- Duration of shock: 1 ms
- Shock strength: 50V/cm
- The electrodes are placed at the bath boundary surfaces
  x = min x and x = max x.



# Sensitivity to the blood vessel wall

— Virtual Electrodes by Externally Applied Electrical Shock

virtual electrodes near small blood vessels without vessel wall model





#### Sensitivity to Conductivity values



#### **Motion of Filaments**



Atrial fibrillation



Figure from Flavio's paper



Filaments (blue curves) dynamics interacting with blood vessels and heart surfaces (green dots) and so virtual electrodes.

Filament data from Rick and Pras



#### Four LEAP scenarios

- 1. Distributed sources for virtual electrodes
- 2. Dynamic motion of the filaments
- 3. Near virtual electrode scroll motion
- 4. Filament tension



#### **Future Plans**

- LEAP defibrillation studies to differentiate among multiple possible mechanisms
- Consider dog or pig models
  - Larger animals
  - Experimental data